# Minimally Invasive Wireless Spinal Cord Stimulation: A Novel Approach for Refractory Angina in Women

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# Abstract

Refractory angina (RA) persists even after thorough treatment for coronary artery disease. In such difficult situations, neuromodulation offers effective alternative management. One such minimally invasive procedure is spinal cord stimulation (SCS), a rapidly evolving therapy in the treatment of pain management. SCS has been in use to control RA and in some reports exhibited beneficiary results. However, several equipment-related complications have been reported, mainly attributed to the bulky implant material and the implantable pulse generator.

Recent advancements in minimally invasive surgical methods and electronics resulted in implantable electrode coupled with nanotechnology-operated antenna. This is the smallest pulse generator in the field of neuromodulation at present.

The equipment in this minimalistic approach involved percutaneous implantation of a single electrode (with embedded microelectronic sensors) at the required anatomical location, operated by means of wireless antenna placed in the vicinity of the implant and moderated by both the patient as well as the clinician. The advantage with the nanoeletrode stimulation include reduced surgical trauma/health care costs/surgical duration and improved cosmetic result, especially in women.

This minimalistic wireless neuromodulation (WNM) has been successful in the man-

agement of chronic pain in failed back surgery syndrome (FBSS), herpetic neuralgia,

complex regional pain syndrome (CRPS), and facial pain. SCS with WNM could increase

the indications in RA and possibly improves the outcome of these patients.

# Keywords

- angina pectoris
- chronic pain
- neuromodulation
- ► wireless
- ► spinal cord stimulation

# Introduction

Conventional therapy and results for stable angina have been directed predominantly on men, while fewer women get enrolled in prospective clinical trials, for various reasons. However, cardiovascular disease (CVD) remains a leading killer in women and death rates due remain higher in women compared with men.<sup>1</sup> Additionally, research has shown that women with stable (defined as retrosternal chest pain associated with exertion or stress and relieved by nitroglycerin or rest) typical angina exhibit more symptoms and functional impairment.<sup>2.3</sup> Manheimer et al defined refractory angina (RA) as "a chronic condition characterized by the presence of angina caused by coronary insufficiency in the presence of coronary artery disease which cannot be controlled by a combination of medical therapy, angioplasty, and coronary bypass surgery. The presence of reversible myocardial ischemia should be clinically established to be the cause of the symptoms. Chronic is defined as a duration of more than 3 months."<sup>4</sup>

Some of the many reasons for failed interventions in RA include anatomy of the coronary arteries, poor response to

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coronary bypass procedures or angioplasty, existing comorbidities, and combination of these factors.<sup>4-6</sup>

Canadian health statistics disclose that ~500,000 Canadians suffer from RA<sup>7</sup> while the American reports estimated that 600,000 to 1.8 million people have RA, with new annual addition of 75,000 patients.<sup>8,9</sup>

European studies reported annual incidence of 30,000 to 50,000 new cases.<sup>4,10</sup> On the other hand, the United Kingdom estimated only 16,500 new cases per year in England and as such specific figures for the United Kingdom could not be defined.<sup>11,12</sup>

These patients suffer from severe pain in the chest resulting in frequent hospitalizations leading to higher health care costs and reduced health-related quality of life (HRQoL) reflecting an increased burden on the society.<sup>4,13</sup>

Multiple options are available to control the symptoms that include medications, sympathectomy, behavior therapy, neuromodulation methods including ganglion blocks, nerve blocks, and spinal cord stimulation (SCS).<sup>14-16</sup>

SCS mediates its effects by epidural stimulation which produces pain relief, reduced sympathetic tone, low myocardial oxygen perfusion, and increased microcirculation in the coronaries thereby controlling myocardial ischemia.<sup>17</sup>

#### Spinal Cord Stimulation in Angina Pectoris

SCS stimulates the dorsal columns and reduces transmission of nociceptive impulses along the spinothalamic tracts modulating several neurochemicals like  $\beta$ -aminobutyric acid (GABA) and  $\beta$ -endorphins with a resultant decrease in myocardial oxygen consumption. Several studies have established the effect of epidural SCS on sympathetic nervous system leading to reduced myocardial oxygen demands.<sup>18-20</sup> SCS also improves homogenization of myocardial blood flow by improving coronary microvasculature dynamics.<sup>21,22</sup>

Additionally, SCS also modifies the capacity of intrinsic cardiac neuronal activity to facilitate relief from angina<sup>23</sup> while the excitatory neuronal effects get suppressed during stimulation.

There is general consensus supported by systematic reviews as well as meta-analyses that SCS can alleviate angina symptoms and improve functional status without increasing mortality and morbidity.<sup>24,25</sup>

The physiological basis for neuromodulation in angina pectoris is as follows:

In 1975 Anpthorp et al demonstrated that sectioning of sympathetic nervous supply provided relief in 75% of patients with angina.<sup>26</sup> Melzack and Wall later demonstrated gate control theory for pain based on the proposal that pain was conducted by small nociceptive c-fibers in the spinal cord.<sup>27</sup> It took a couple of decades to demonstrate the benefits of SCS in chronic RA, when Murphy and Giles stimulated the spinothalamic tracts by placing a nerve stimulator connected to an epidural electrode pole to stimulate the dorsal horn interneurons with a low amplitude current.<sup>28</sup> This stimulation inhibited nociceptive signals, producing pain relief.

In due course, several randomized studies supported the utility of neuromodulation in peripheral vascular disease (PVD) as well as RA<sup>29-33</sup> albeit in smaller samples.<sup>25,34</sup>

Pan et al demonstrated the safety and efficacy of SCS in RA, wherein SCS improved exercise time, decreased medication, as well as disease perception with significant improvements in QoL.<sup>34</sup>

Historically, however, SCS in its conventional equipment form, has not been devoid of complications or limitations utilizing an implantable battery. Several patients have failed the stimulation and the SCS systems have had a long history of severe adverse events, mainly attributable to the implantable pulse generator (IPG) battery.<sup>35,36</sup> A significant number of patients, almost 50%, reportedly have failed the SCS trial,<sup>35-37</sup> while additional failures came from complications contributed by the migration/fracture of the electrodes. IPG failures and complications added to this failed SCS therapy. Postoperative infection, hemorrhage, and painful operative wounds were frequently reported with IPG and its extension wires. Additionally, SCS cannot provide adequate pain relief in some anatomical locations in its conventional form due to its stimulation parameters.<sup>35-38</sup>

Several modifications to the SCS equipment have reduced adverse events, in an effort to improve the efficacy of the therapy, thus increasing the indications for neuromodulation.<sup>39</sup> Some of these modifications include percutaneous implantation techniques, smaller/compact batteries with increased life of pulse generators, rechargeable batteries, and innovative anchoring methods. Additional advancement has been derived from the improvements in the application of nanomaterials and wireless power transfer techniques for clinical purpose.

## The Wireless Neuromodulation Apparatus

This innovative implant has miniature components embedded in a single implant. The power transfer techniques utilize microantenna incorporated in to the electrode and activated by wireless approach via an externally placed power source.

## Implantable Neural Stimulator (INS)

This stimulator is composed of an encasing sheath with the stimulating electrode array, which delivers electrical pulses to the target and an antenna-1 configured to receive the energy-input from an externally placed antenna-2 through electric radiative coupling. The second antenna remains physically away from the implant, INS lead, and communicates with the antenna-1 by circuits designed to generate electrical pulses meant for stimulation of the target (**– Fig. 1a, b**).

The microimplant wireless power generator (WPG) on antenna-1 delivers the appropriate stimulation impulses, has 800 to 1350  $\mu$ m diameter, a very small compact size compared with the conventional SCS-IPG. The INS can have a variety of leads (with 4 or 8 contacts). Electrode can be cylinder or paddle type (**> Fig. 1a**). The contacts are kept at a 3 mm distance apart on the electrode (**> Fig. 1b**).

Patient receives the implant, one or more, according to the required stimulation parameters and the target locations which gets coupled with the wireless receiver (**>Fig. 2**). The WPG remains in the vicinity of this INS, outside the patient body, as the power source, worn by the patient over a single layer of cloth (**>Fig. 3**). Thus, there is only one electrode, a passive and wirelessly activated implant, placed inside the

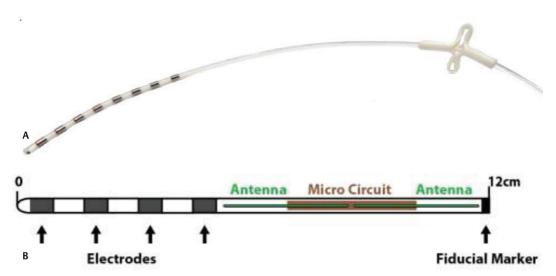


Fig. 1 The nanoelectrode with introducer. (b) The Stimwave implantable neural stimulator (property of Stimwave Technologies).

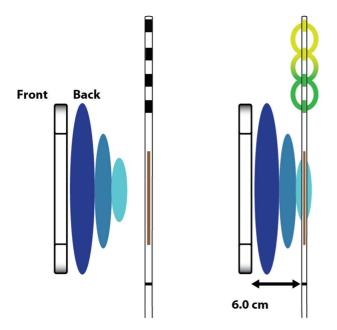


Fig. 2 Neurostimulator receiver (property of Stimwave Technologies).

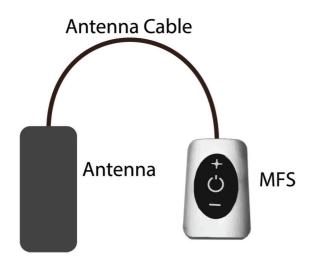


Fig. 3 External pulse generator (property of Stimwave Technologies).

patient, without any connecting wires, anchors, and IPG. The INS receives the desired stimulation via a radiofrequency (RF) transmitting antenna inside the WPG. The implant utilizes RF energy of 915 MHz to transfer the energy and the stimulation parameters as indicated for the patient.

Thus the only implanted component is a miniature electrode. This is passive electrically, and is operated by the transmitter in an external pulse generator (EPG), worn by the patient over a single layer of cloth. The INS receives the desired range of stimulation from the EPG via a radiofrequency (RF) transmitting antenna (**-Fig. 4**). The implant and the EPG use RF energy at 915 MHz to transfer power and selected stimulation parameters depending upon the patient's condition and appropriate clinical use.<sup>40</sup>

## Discussion

SCS has been reported to be a safe therapeutic option for clinical application in patients with refractory angina. However, the conventional device had serious adverse events in several studies on SCS.<sup>24,25,37,38,41-43</sup> Traditional SCS has multiple implantable components that require multiple incisions and several anchors to keep the accessories in position. The procedure also requires longer time and possibly longer exposure to intraoperative radiation.

The IPG location is usually on the front of the chest (below clavicle) or in the abdomen/back, often seen as a bump with an overlying scar. In women, this may not be an acceptable cosmetic result.

On the other hand, wireless SCS (WSCS) requires only one device to be placed inside the patient and by percutaneous techniques. Implantation of the electrode with inbuilt miniature antenna is very minimalistic in surgical approach since WSCS does not require accessories to be implanted. For the same reason, revision procedures would be less invasive and explantation of the device would be much simpler compared with the traditional SCS equipment (**~ Table 1**).

WSCS avoids the tethering effects due to connection cables/ anchors and thus has less chances for lead migration, fracture, or displacement resulting in failures and complications.<sup>44</sup>

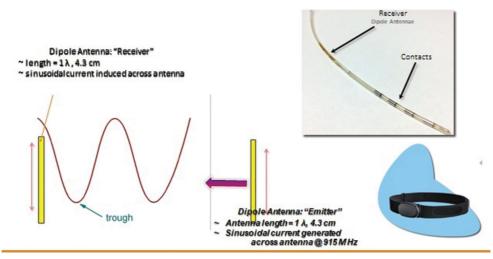


Fig. 4 Nano-electronics and mechanisms involved in the minimally invasive wireless neuromodulation.

Variable	Wireless SCS	Nonwireless SCS						
Implants	Only electrodes	Electrodes						
	Anchor	Implantable pulse generator						
		Connections cables						
		Multiple anchors						
Incisions	One/two	Multiple						
Bulk	Electrodes only	Heavy due to IPG						
Trial	Not required	Required						
Scars	Small, single mostly	Multiple						

Table 1	Differences	between wire	eless and	nonwirel	ess spinal
cord stin	nulation (SCS	)			

Large-scale multicenter randomized studies are being currently undertaken to establish grounds for routine use of this simple, minimally invasive device.<sup>48</sup> WSCS has the potential to reduce health care costs, hospital stay, and surgical trauma with improved acceptance from patients since the cosmetic result is much superior. Especially in patients with multiple comorbidities and limited life expectancy, this miniature device offers a better option to control chronic pain. RA is a condition that predominantly affects elderly people who have severe coexisting morbid conditions. WSCS can be the most appropriate choice to control their symptoms especially with a background of microvascular ischemia.

Table 2	Experience	with	n wireless	s neuromod	u	lation	in	women

	Diagnosis	Age	Procedure	Outcome	Ref.
		(y)			
1.	CRPS	47	PNS Radial and Median nerves	Relief	47
2.	Discopathy	67	SCS at T9	Relief	45
3.	FBSS	33	SCS at T9	Relief	45
4.	ON	58	Occipital nerve Stimulation	Relief	46
5.	FBSS 34 patients		SCS	Relief	48

Abbreviations: CRPS, complex regional pain syndrome; FBSS, failed back surgery syndrome; ON, occipital neuralgia; PNS, peripheral nerve stimulation; SCS, spinal cord stimulation.

Wireless device from Stimwave (Stimwave Technologies, Fort Lauderdale, Miami, Florida) belongs to an advanced version of wireless technology and is programmable between 0 and 10,000 Hz frequency. It has been approved by FDA for SCS and peripheral nerve stimulation for several years now.

In several case illustrations, WSCS and wireless PNS provided effective pain relief. The technology demonstrated safety and feasibility in many instances with results comparable to the therapeutic efficacy of traditional SCS.<sup>45-48</sup> Experience with wireless neuromodulation in a variety of chronic pain syndromes has been published in many reports (**– Table 2**).

#### **Conflict of Interest**

Dr. Tyler Perryman reports that he is Chairman and CEO of Stimwave Technologies Incorporated. In addition, Dr. Tyler Perryman has a patent 1. US9409029B2 Remote RF power system with low profile transmitting antenna 2. US9254393B2. Wearable antenna assembly 3. US9220897B2. Implantable lead 4. US9199089B2. Remote control of power or polarity selection for a neural stimulator. 5. US8849412B2. Microwave field stimulator. 6. US8903502B2. Methods and devices for modulating excitable tissue of the exiting spinal nerves. 7. US9409030B2. Neural stimulator system. 8. US15228715. Remote rf power system with low profile transmitting antenna. 9. US9522270B2. Circuit for an implantable device issued. Dr. Slavin reports and confirms being a consultant/advisor for Abbott, Biotronik, Boston Scientific, Medtronic, Neuramodix, Nevro, Nuvectra, SPR, Stimwave, and Thermaquil, and has minor ownership or ownership option in Higgs Boson, Neuramodix, Stimwave, Thermaquil, and Vycor Medical.

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